

Europäisches Patentamt European Patent Office Office européen des brevets



EP 0 797 952 A1

EUROPEAN PATENT APPLICATION

(12)

(43) Date of publication:

01.10.1997 Bulletin 1997/40

(51) Int CLS: A61B 8/08, A61B 6/00

(11)

(21) Application number: 97302116.5

(22) Date of filing: 26.03.1997

(84) Designated Contracting States: DE FR GB IT NL

(30) Priority: 26.03.1996 US 622030

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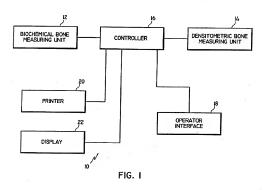
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(54) System for assessing bone characteristics

(57) A system or method for determining bone characteristic data is provided. The system combines a biochemical bone measuring unit (12) with a densitometric bone measuring unit (14) to determine the bone char-

acteristic data. Once the bone characteristic data is ascertained, a determination of whether bone formation or bone resorption is occurring is made and future bone characteristics can be projected.



Description

BACKGROUND

1. Field of the Invention

The present invention relates to systems for assessing bone characteristics. More particularly, the present invention relates to a system that performs biochemical and densitometric assessments of bone material to provide practitioners with bone characteristic data for evaluation of a patient's bone material for diagnosis and management of bone related disease.

2. Description of the Related Art

The diagnosis and management of bone related diseases, such as osteoporosis, hypically requires information about bone turnover and bone mass, Determinations of bone turnover have historically bone per-atorised utilizing standard serum and/or urine isboratory tests including astelling eaction/recentinine, hydroxyproline, allsaline phosphatase and/or catecoalcin/hone growth protein utilizing standard high pressure liquid chromatography (HPLC) techniques. To litustrate, as whenever hore formation occurs (eactium deposition) or bone resorption occurs (eactium the body which elevate the presence of cartain indicators in the blood and urine suggesting changes in the eacticum/hore minerial status. 30

Recently, several new bone specific assays have been developed which enable bloom tumover to be evaluated with an ELISA/EMIT immunoassy formats can be found in U.S. Patent Nos. \$373,686, 5,20,370, \$,300,434 stand \$1,40,103. The labeling for the new assays utilize a blochemical marker to quantify bone resorption and/or formation and permit a trained practitioner to assess bone tumover.

Bone mass determinations, on the other hand, have been traditionally performed by using various x-ray based techniques including single and dualphoton absorptiometry (SPA and DPA), quantitative computed tomography (QCT), and dual-energy absorptiometry (DXA).

To roduce the time necessary to determine it bone recorption or formation is occurring and to permit a practitioner to project future bone characteristics, a system which combines a biochemical bone measuring system that measures, for example, bone tumover, with a denseation to the company of the combine of the company of the combine of the combine

Further, the X-ray based equipment emits ionized radiation in the form of x-rays and requires a licensic form of x-rays and requires a licensic sequipment. In addition, this equipment is structurally large and constructed to house, for example, an x-ray source and an x-ray detector, and provides a large table area to position the

patient for examination. As a result, such x-ray based equipment occupies a large floor area. In addition, since x-rays are emitted by such equipment, certain safety precautions must be followed to limit human exposure to the emitted rays.

High frequency ultrasound has recently become an alternative technique for determining preliminary assessments of bone status. Measuring the bone density with ultrasound is currently more desirable over some of the above mentioned techniques since there is no ionizing radiation in the form of x-rays produced by ultrasound. As a result, a licensed x-ray technician does not have to be employed to operate the ultrasonic measuring equipment and the environment where the instrument is located and operated is not strictly regulated. In addition, ultrasonic measuring equipment can be manufactured significantly smaller in size and weight than the above-mentioned x-ray type bone density measurement equipment and is suitable for installation in private offices or medical facilities where space is typically at a premium

The parameters that can be determined using ultrasound include the speed-of-sound, the attenuation of the ultrasound signal and/or combinations of the above as it penetrates bone and tissue. These parameters provide general characteristics relating to bone density and the risk of fluver fracture.

Although the above described assay techniques provide a practitioner with information regarding the rate of bone resorption or formation, the results from such techniques are of limited value unless a baseline level of bone mass can also be established. Measuring bone density provides practitioners with baseline bone density information and after successive measurements over a period of time, e.g., one year, may also permit the practitioner to determine if bone resorption or bone formation is occurring. However, this process takes a period of time (nominally, approximately one year) to determine if there is bone resorption or formation occurring. Biochemical markers which evaluate physiological status directly are capable of evaluating the change in the amount of bone formation or resorption, for example, in response to therapy, in a matter of months. Thus, to quickly and accurately obtain an assessment of bone formation or resorption a practitioner typically utilizes both measurements to obtain the necessary bone characteristic data

Thus, a need exists for a bone measuring system capable of performing various types of assessments of bone material and providing a practitioner with bone characteristic data in the form of, for example, graphical display results, to permit the practitioner to diagnose and manage bone related disease.

A need also exists for a compact and inexpensive system that may be installed in a practitioner's office or like location and that reduces the time necessary to determine bone resorption or formation and to permit a practitioner to diagnose and manage bone related dis-

SUMMARY

The present invention provides a biochemical bone measuring unit and dentelmetric bone measuring unit and dentelmetric bone measuring unit to form a bone measuring system that performs biochemical and densitometric assessements of bone material. The system of the present invention provides practitioners with bone characteristic data to evaluate bone status, and some instances provides a prognosia as to future bone characteristics on a comble the practitions or harage bone related disease.

In one embodiment, the system of the present invention combines the biochemical bone measuring unit and the densitometric bone measuring unit into a single housing which is compact and capable of being installed in a matilition of soffice.

In an alternative embodiment, the densitometric and biochemical units are connocted to each other via standard data communication circuitry and either the densitometric bone measuring unit or the biochemical bone measuring unit has a controller that combines the measurements from each unit to provide practitioners with the bone characteristic density.

In another alternative embodiment, the blochemical bone measuring unit and the densitometric bone measuring unit may be individual units that exparately perform blochemical and densitometric bone assessments. The results of the individual assessments can be manually or automatically combined to provide practitioners with the bone characteristic feets.

In another alternative embodiment, the biochemical bone measuring unit and the densitometric bone measuring unit may be individual units that separately per- 35 form biochemical and densitometric bone assessments and transfer data from such assessments to a separate personal computer. The personal computer combines the measurements from each unit and performs the bone assessment to provide practitioners with the bone 40 characteristic data. In one embodiment, the single unit system includes a housing having a bone mass measurement system and a sample access port, a display mounted to the housing such that a display surface of the display is visible through the housing. Strip reader circuitry is located within the housing and is configured to direct light to a strip sample, to filter light reflected by the strip sample such that at least one predefined color wavelength is permitted to pass, and to detect the filtered light and generate a detected sample signal. The 50 strip reader circuit and the sample access port form the biochemical bone measuring unit (or system). The single unit bone measuring system also includes the densitometric bone measuring unit (or system) positioned within the housing and configured to generate bone 55 mass data. The densitometric bone measuring unit preferably includes a pair of adjustable ultrasonic transducers, and associated encoders and drive mechanisms to

move the transducers. A processor is located within the housing and is coupled to the strip reader circuit and the ultrasonic transducers, the encoders and the transducer drive mechanisms. The processor is provided to receive a detected sample signal from the strip reader circuit and to generate bone turnover data from the detected sample signal. The processor also controls the operation of the ultrasonic transducers and determines bone mass data. The processor then processes the bone tumover data and the bone mass data to determine if bone formation or resorption is occurring (i.e., performs the bone assessment). Once the current bone density and the bone turnover data are ascertained and a determination of whether there is bone formation or resorption is made, then the processor can project future bone characteristics and provide the results on the display or by a printout. Such results may include a graph of bone density verses time, or a listing of bone density values over a period of time.

In an alternative embodiment, the bone measuring system of the present invention is constructed from inclididual components and includes a controller havingmemory and data communication capability, a behavingized bone measuring unit coupled to the controller, and a denellmentatio bone measuring unit coupled to the controller, in this embodiment, the controller performs simfar operations as those described above.

The present invention contemplates different embodiments for the individual biochemical bone measuring unit and the densitometric bone measuring unit. One embodiment of the biochemical bone measuring unit includes a housing having at least one access port adapted to receive a strip sample, or to direct a bodily fluid sample onto one or more strip tests or a receptor pad in the housing, at least one strip sample reading circuit located within the housing and configured to direct light to the strip sample, to filter light reflected by the strip sample so that at least one predefined color wavelength is permitted to pass, and to detect the filtered light and generate a detected sample signal, and a processor located within the housing and coupled to the at least one strip sample reading circuit. The processor is preferably configured to receive the detected sample signal, to generate bone turnover data from the detected sample signal and to display the bone turnover data. The biochemical bone measuring unit may optionally include a display mounted to the housing so that a display surface of the display is visible through the housing. The housing can be configured to be hand-held having dimensions similar to those of, for example, a hand-held calculator.

The side sample reading circuit uses a light entitler source, an optical filter and a light receiving element or read a cobor marker on a side sample containing the immunosassy. The light entiting source is configured to 6 emit light (e.g., laser, incundescent, fluorescent, light entitler dicholo lower the side sample and the optical filter is configured to permit predefined color waveneaghter effected from a sample portion of the strip configured to permit predefined color wavemental reading to the configuration. In an attemative embodiment, the strip sample includes a reference portion in addition to the sample portions, and the strip sample reading circuit includes a second optical filter and a second light detecting element.
A second optical filter and a second light detecting element.
A second optical signal is configured to pass predefined
corr wavelengths of light reflexed from the reference
portion of the single sample and the second light detecting
element receives the filtered reflexed light and goverelement signal provides a control value as an indeated remos signal provides a control value as an indeation of the suality of the strip sample.

In another alternative embodiment, the strip sample reading circuit includes an optical filter positioned in front of a light source and the light emitted from the strip sample passes through a second filter so that fluorescent light from the sample impinges a light detecting alement and generates a signal for transfer to the proc-

The deneitometric bone measuring unit may be, for example, an utressound based unit or an x-ray based unit. One embodiment for an utrasound bone measur-ray from unit includes a pair of utrasorio transducers which are movable relative to each other, associated drive mechanism that moves the transducers, and encoder circuity and temperature sensors to measure transducer of characteristics for calculation of bone density. A rack and pinion type of drive mechanism as committed to the control of the c

The present invention also provides a method for determining and displaying bone characteristic data. The method fellouses the eleps of readings attip sample 4b by directing light toward the etrip sample and detecting light toward the etrip sample and detecting light reflected or entitled from the step sample and generating signal data indicative of a concentration of a bit-cohemical enalytic or a combination of a shape and defining bone turnover data associated with a patient, dot-taining bone density data for the patient, and determining whether bone formation or rescription is occurring based on the bone turnover data. The determinations of turnover data and the bone turnover data. The determinations of bone for unrover data. The determinations of bone for unrover data. The determinations of bone for unrover and bone density data and the bone turnover data. The determinations of bone for unrover and bone density can be graphically displayed on a computer monitor in the form of charts and graphs.

BRIEF DESCRIPTION OF THE DRAWINGS

Preferred embodiments of the invention are described hereinbelow with reference to the drawings wherein:

- Fig. 1 is a block diagram of one embodiment of a bone measuring system according to the present invention;
- Fig. 2 is a block diagram of an alternative embodiment of the bone measuring system according to the present invention:
- Fig. 3 is a block diagram of the components of a biochemical bone measuring unit of the system of Figs. 1 and 2 illustrating an exemplary strip sample reading circuit;
- Fig. 4 is a block diagram of an alternative embodiment of the components of a biochemical bone measuring unit of the system of Figs. 1 and 2, illustrating multiple strip sample reading circuits;
- Fig. 5 is a block diagram of an alternative embodiment of the components of a blochemical bone measuring unto the system of Figs. 1 and 2, illustrating a strip sample reading circuit configured to read two markers on a strip sample;
- Fig. 6 is a block diagram of an alternative embodiment of the components of a biochemical bone measuring unit of the system of Figs. 1 and 2, illustrating a strip sample reading circuit configured to use fluorescent light to read a strip sample;
 - Fig. 7 is a block diagram of an alternative embodiment of the components of a biochemical bone measuring unit of the system of Figs. 1 and 2, illustrating a disposable strip sample and strip sample reading circuit;
 - Fig. 8 is a block diagram of the system of the present invention, and illustrating a biochemical bone measuring unit and ultrasound densitometric bone measuring unit connected to the controller;
 - Fig. 9 is a perspective view of one embodiment of an integral bone measuring system according to the present invention, and illustrating the biochemical bone measuring unit and the densitometric bone measuring unit in a compact housing;
- Fig. 10 is a schematic view of a patient's foot positioned in the bone measuring system of Fig. 9, and illustrating a foot bridge for maintaining the position of the foot;
 - Fig. 11 is a front elevational view of the foot bridge of Fig. 10;
 - Fig. 12 is a front elevational view of a portion of the internal components of the bone measuring system of Fig. 9, and illustrating a pair of transducer assem-

blies movable relative to each other, and associated drive mechanisms for moving the transducers,

Fig. 13 is a perspective view of a biochemical bone measuring unit according to the present invention;

Fig. 14 is a block diagram of an atternative embodiment of the bone measuring system according to the present invention:

Fig. 15 is a block diagram of an alternative embodiment of the bone measuring system according to the present invention, and illustrating an utrasonic densitometric bone measuring unit and a biochemical bone measuring unit coupled to a computer by a communication Interface.

Fig. 16 is a block clagram of another alternative embodiment of the bone measuring system of the present invention, and illustrating an x-ray based densitioneriric bone measuring unit and a biochemical bone measuring unit coupled to a computer by the serial communication interface; and

Figs. 17-19 are exemplary computer generated ²⁵ graphical displays, illustrating baseline, monitoring/ follow-up and dynamic displays for providing a practitioner with graphical results of the bone assessments.

DETAILED DESCRIPTION

The bone measuring system of the present invention combines a bichemical bone measuring unit and a densitometric bone measuring unit to form a system that performs blochemical and densitometric assessments of bone material. Such assessments provide practitioner with bone characteristic data to evaluate bone status, and in eome instance, to provide a progness of future bene formation or resorption.

In the embodiments discussed hereinbolow, the bone characteristic data includes bone turnover data which is measured by the biochemical bone measuring unit, and bone mass data which is measured by the densitionalitie bone measuring unit.

Blochemical assessments of bone characteristics can be made by detecting characteristics from, for example, an assay based stip sample. The stip sample is typically the result of a cumulative in-vitro diagnostic stip test performed on a bodily fluid sample such as 60 blood or urine. However, other techniques or methods may also be utilized for blochemical assessments. For example, the techniques contemplated include a solid-phase immunessay technique, as western bidding technique and fluorescent microscopy technique. Various 5/psec of assess, such as chemical, enzymatic, and immunochemical assays, may be used on the stip sammune, Chemical assays may detect, for example, phos-

phorous and/or calcium. Enzymatic assays may detect, for example, the enzyme action of alkaline phosphatase. Immunochemical assays may detect biologic compounds by monoclonal or polyclonal antibodies or specific receptor proteins.

The strip test incorporates one or more markers evaluating bone resorption, bone formation or a combination of both attached to a strip backing and a color marker bound to the bone formation or resorption markers. The strip test may be configured in various shapes including, for example, rectangular, square, circular, and triangular shapes. The strip test also includes receptor pads used to absorb bodily fluids. Preferably, the strip test employs a monoclonal or polyclonal antibody or antibodies to capture and detect an analyte. For example, bone-specific alkaline phosphatase, osteocalcin, or propeptides of type-I procollagen can be used as markers for determining bone formation, and/or telopeptide of type-I collagen, pyridinoline, deoxypyridinoline, or hydroxyproline can be used as markers for determining bone resorption. These antibodies, can be pre-applied to the strip test backing surface. A strip sample typically includes the strip test and the bodily fluid. Preferably, when a bodily fluid sample is applied to the strip test. the strip sample provides an optical scaling response proportional to the concentration of the analyte on the strip sample. The optical scale assignment provides quantitative information about the amount of analyte on the strip sample which Indicates whether bone resorption or formation is occurring depending upon which of the markers are attached to the strip test backing.

Referring to Fig. 1, a block diagram of an alternative embodiment of the bone measuring system 10 of the present invention is shown. The bone measuring system 10 includes a biochemical bone measuring unit 12 and a densitometric bone measuring unit 14 connected to a controller 16. The blochemical bone measuring unit 12 provides the controller 16 with detected signals representing, for example, bone tumover data. The densitometric bone measuring unit 14 provides the controller 16 with detected signals representing, for example. bone density data. The controller 16 then processes the signals from each unit and determines, for example, whether bone formation or resorption is occurring. After the controller determines if bone formation or resorbtion is occurring, results of the assessment can be provided via printer 20 and paper port 21, or display 22. An operator interface 18 is connected to controller 16 to permit user interaction with the controller.

Referring to Fig. 2, a block diagram of an alternative embodinem of the bone measuring system of the prosent invertion is shown. In this embodiment, the bone measuring system 10 includes a biochemical bone measuring unt 12 connected to a densitionetric bone 6 measuring unt 14 which includes the controller 16 that receives information from the biochemical bone measuring unit as well as the densitionetric bone measuring unit as

Referring to Fig. 3, the bicchemical bone measuring unit 12 of the system 10 of the present invention includes strip sample reading circuit 24 that measures the optical scaling response of the strip sample. The strip sample reading circuit 24 includes a light source 26 which emits light towards a sample strip 28 which is inserted into a access port 29, seen in Fig. 9. Suitable light sources include light-emitting and laser diodes, and incandescent and fluorescent lamps. Light reflected from the sample strip 28 is filtered by optical filter 30 and impinges light detector 32. A suitable optical filter is a color filter which permits predetermined color wavelengths to pass therethrough. For example, the optical filter 30 may be a polarized lens disposed at a predetermined angle to permit certain wavelengths to pass. The output of the light detector may be an analog or digital signal which is transferred to the controller 16. A suitable light detector is a photodiode

If the output of the light detector is an analog signal then the controller 16 may include an analog-to-digital converter to convert the analog detector signal to a digital format for subsequent processing. Alternatively, the light detector may include an analog-to-digital converter and drive circultry which performs the signal conversion and transfers the signal conversion and transfers the signal to processor.

Fig. 4 shows an embodiment where the biochemical bone measuring unit 12 includes a plurality of strip sample reading circuits 24 aligned with a plurality of strip samples and connected to the controller 16. In this embodiment, the plurality of strip samples can be read and 30 the information obtained therefrom can be used to determine bone turnover. For example, one strip test may have bone formation markers attached thereto and the strip sample represents bone tormation, and another strip test may have bone resorption markers attached 35 thereto and the strip sample represents bone resorption. The ratio between the measured value from the bone formation strip test and the measured value from the bone resorption strip test provides bone tumover data. When the bodily fluids sample ie urine, the measured bone formation and/or resorption values may vary depending upon the time period between urine secretions by the patient. To compensate for such variations a creatinine normalization technique may be implemented. Creatinine normalization provides a baseline marker for 45 urine concentration and if the creatinine concentration level is high the bone marker concentration level may be high resulting in an inaccurate estimate of bone formation or resorption. To compensate for variations in bone termation and/or resorption values, a ratio of the bone marker concentration level to the creatinine concentration level is obtained to determine the extent to which bone formation or resoration is occurring. To determine the creatinine concentration level a color marker that binds with creatinine can be attached to a strip test 55 backing and when combined with the urine strip sample. can then be measured by the strip sample reading circuit. The controller in the biochemical bone measuring

unit can then determine the ratio of bone marker concentration level to the creatinine concentration level to more accurately determine bone turnover.

Referring to Fig. 5, an alternative embodiment of the strip sample reading circuit 24 is provided. In this embodiment, a second optical filter 54, which is similar to optical titler 30, and a second light detector 86 are provided to read a reference sample portion on the strip sample 28 simultaneously when reading the portion of the strip sample to be tested. The reference sample provides a known reflectance value which may be utilized to perform a system calibration or to verify the quality of the strip sample being measured (e.g., to determine it the strip sample is stale).

Fig. 6 shows an embodiment of the bono measuring unit 12 having a fluorecont light source 26 that emits light through filter 31 toward the strip sample. The filter 31 is used to filter the light trom the source 25 so that only excitation light passes therethrough. Filter 30 is used to filter the fight metted from the strip sample so that only fluorescent light passes therethrough. In this embodiment, the fluorescent microscopy technique is used to perform the observable strip to the fluorescent microscopy technique is used to perform the biochemical assessment of the bone material.

Fig. 7 shows an embodiment of the bone measuring unit 12 having a disposable reader portion 25 that includes strip sample reading circuit 24 and strip sample 28. In this embodiment, the strip sample is internal to the unit 12 and a bodily fluid sample is deposited onto the strip test. After a sufficient time has elapsed to allow the analytes in the sample to interact with the strip test. the strip sample reading circuit is activated to measure. for example, the concentration of analytes. After a bodily fluid sample is tested, the disposable reader portion 25 is removed from the unit and a new disposable reader portion is inserted for testing another bodily fluid sample. as seen in Fig. 13. As discussed above, the controller 16 processes the detected signals from the strip sample reading circuit and determines bone turnover. As noted, the controller 16 can format the detected signals for transmission to, for example, the densitometric bone measuring unit 14 via communication port 21. Known data transmission techniques may be used to transfer the data from the biochemical bone measuring unit.

During operation of the biochemical bone measuring up to the point 12 seen in Fig. 3, the bone measuring system 10 can be turned on by depressing button 38 and them a strip sample 28 is inserted find so trip access por 29. The measurement function can then be activated by depressing button 40. When the measurement function is activated, the controller 16 sends a signal to light source 28 which emits light toward the strip sample 38. Light which impringes the strip sample is at least partially reflected toward optical filter 30 which permits predefined wavelengths of light reflected 10 with cettor 32. The light deslocts from generatios a sample detected signal representing the color effectance value of the reflected light and representing the color effectance value of the reflected light and transfers the

sample deflorted signal to the controller 16. The controller 15 receives the sample deflorted signal and deflermines the bone turnover rate. For example, as the color increases the sample deflorted signal decreases indicating increased none turnover, or as the color decrease es the sample deflorted signal increases indicating decreased bone turnover. The resulting bone turnover data may then be displayed by display 22 or provided as a hard con by the portions 20

In the embodiment of Fig. 5, the reflected light from 10 the strip sample is also filtered by optical filter 34 and is passed to the light detector 36. The light detector 36 responds by generating a reference detected signal which is related to the color detected. The reference detected signal is then transferred to the controller 16 and converted to a digital format using for example, an analogto-digital converter. Controller 16 receives the reference signal and compares the reference signal to a control reflectance value stored in the controller memory. For example, as the difference between the reterence signal and the sample detected signal increases the sample detected signal decreases indicating increased bone turnover, or as the difference between the reference signal and the sample detected signal decreases the sample detected signal increases indicating decreased 25 bone turnover. If the reference value is not equal to or within a predefined tolerance (e.g., ± 10 percent) of the control reflectance value, the controller may then discard the sample detected signal generated by light detector 32 and discontinue the measurement procedure. Further, the controller may display that a error has occurred in the biochemical bone measuring unit 12, or that the strip sample 28 is unsuitable for testing. If the reference value is equal to or within the predefined tolerance then the processor continues the measurement 35 procedure.

The above-described blochemical bone measuring unit 12 performs the biochemical assessment of bone characteristics. As noted above, the system 10 of the present invention performs biochemical and densitometric assessments of bone characteristics.

The densitometric bone measuring unit 14 may use ultrasound for measure brondband ultrasound rate unitrasound research profits of ultrasound research profits of the profit

Fig. 8 is a block diagram of the bone measuring sys-

tem 10 with a biochemical bone measuring unit 12 and an ultrasound bone measuring unit 14. The ultrasound bone measuring unit 14 generally includes a pair of transducer assemblies 50 connected to a transducer drive mechanism 52 that automatically positions the transducer assemblies 50 against a body part of a patient, e.g. the patient's heel, with sufficient pressure to insure ultrasonic coupling. A position encoder 54 is used to determine the position of the transducer assemblies 50. A temperature sensor 56 is provided to improve the accuracy of the position encoder measurements and to correct for temperature dependent inaccuracies in the ultrasound measurements. A more detailed description of an ultrasound densitometric bone measuring unit is described in copending application Serial No. 08/477,580, filed June 7, 1995, which is incorporated herein in its entirety by reference.

Reterring to Fig. 9, a perspective view of an integral bone measuring system 10 is shown. In this embodiment, the system 10 has a housing 60 that is configured to firmly support, for example, a patient's foot for the uttrasound bone measurement. Figs. 9-11 illustrate the foot support for the system 10. However, ultrasound bone measurements of other body portions of a patient outh as the footenam, wrist or phalanges, may be made

In the embodiment of Figs, 8-11, the housing 60 hae a base portion 60a and a support portion 60b. The support portion is configured to receive a patient's and includes support structures used to position and restrain the and lower leg in a predefined position which provides optimum coupling of ultrasonic transducer energy with the patient's ankle. The support portion 60b of housing 60 includes a well 62 configured as a universal support which receives large adult size teet as well as small children's feet, and bridge brackets 64 and 66 which include channels 68. The channels 68 are angled at a predefined angle (a) with respect to the base 62a of the well so as to ensure stable restraint of the and leg of the patient. Preferably, the predefined angle is 55 degrees. Transducer ports 70 are located on the sides walls of the well 62, as seen in Fig. 9.

Referring to Fig. 10, a restraint member 80 has two holeopordent subassemblies, namely a shir guide assembly 84. The shir guide assembly 82 and a bridge assembly 84. The shir guide assembly 82 includes a plastic modied form 88 professional statements of the shirt o

The modeled form 86 includes whin restraint section 90 which restraint, supports, and centers the bilb against the confound form lining 80 using a facilities starp 92 placed around the call muscle. The start belief starp 92 placed around the call muscle in the start belief starp 92 can be adjusted to secure the modeled from 86 comfortably around the shin region. The shin restraint section 90 of the shin guide assembly 92 catefact supward from an instea support section 94 at an ordefined

angle with respect to the well bottom 62a. Preferably, the predefined angle is about 95 degrees.

Referring again to Fig. 10, the front of the is restrained from letters tratified by a contraint continue.

Referring again to Fig. 10, the front of the is restained from literial rotation by a restainat section 50 of extending from the lower part of the instep support section 94 tewards the loss. As seen in Fig. 10, the restaint section 56 has a contioused foem lining 98 which is provided to properly center the fort of the as the moisdor form 68 is lowered to align with the correct width of the patients. Because the michanes of the also varies the enally, the height of the restaint section 96 is typically greater near the instep than near the front of the.

Referring 16 Figs. 10 and 11, the bridge assembly 84 is configured for mounting on opposing sides of the morbid form 86 and for using slide blocks 100. The bridge assembly 84 is provided or taken the shi nguide assembly 82 to the housing 60 and to properly sligh and maintain the peating of the provided real slight and maintain the peating of the provided real slight the slide blocks 100 are inserted into corresponding channels 68 in breakets 64 and 66 octonising from the support portion 60b of housing 60. The preferred 55 degree angle of the channels 68 facilities proper contact between the bridge assembly 64 and the instep area of different size lest, see will as, sufficient different into the size of the size of the size of match and the size of the size of match and the size of the size of match and enter varying widths of the lewer.

Referring to Fig. 11, the channels 68 are lined with strips of repeating infrangular raches teach 102 executed to each bracket 64 and 68. The slide blocks 100 have matching mitches teach 102 in experision with the twest 102 excurred to the brackets. This configuration is similar 102 asset with extended to a pawl and rache mechanism. When the slide blocks 100 are inserted into the channels 68, the ratchelling action between select the 20 and 104 allows the slide blocks 100 to latch at one of multiple levels to the bridge brack-30 test 64 and 68 so as to permit selective adjustment of the shin guide assembly can be adjusted to provide a comfortably fit for any size, while maintaining the proper restraint of the patient's and size, while maintaining the proper restraint of

To facilitate release of the matting ratchet tooth 102 and 104, the ratchet teel 104 are prefeably attached to spring assembly 110 which includes leaf spring 106 mounted to the base of the skide blocks 100. To release the ratchet leaft, an operator squeezes logather two right dibrackets 106 of spring assembly 110 which are attached to the free ends of the springs 106. When an operator's requeeze the brackets together, ratchet teels 104 are clear of the teels 105 are only the teels 105 are the

Shin guide assembly 82 may be conveniently stored tor transport of the restraint member 80 by sliding the slide blocks 100 into a lowest position in the channels so

Referring now to Fig. 12, transducer drive mechanism 52 automatically positions transducer assemblies

50 against the patient's hool with sufficient pressure to insure ultrasonic coupling. Preterably, each transducer assembly 50 includes a transducer 120, an acoustical delay line 122 and a coupling pad 124.

Based on the quality of the signals received from the transducer assemblies 50, he coupling pressure is modified under control of controller 16, seen in Fig. 8, to insure proper operation. The quality of the signals received is determined at least in part according to the strength of the signals (i.e., the signal amplitude) and the positional datas of the transducers with respect to the patient. As noted above, the position encoder 54 is utilized to determine the position of the transducers.

The transducers 120 are mounted to respective carriages 126 and are configured to slide independently along a lateral-medial axis. Respective compression springs 128 attached to the carriages 128 apply opposing lateral forces towards the context of the . In this configuration, the carriaged/pring assembly is tree floating and will center itself on the with equal pressure on both sides.

An extension spring 130 applies the Initial pressure when the coupling pade 124 reach the patients. To act just the pressure in small increments, a stepper motor 132 with, for example, a resk can pinch mechanism 134 will move a finite number of steps and compress the compression prings 128 statished to the respective carriages 126. The compression springs 128 will put ill mespective transducer assemblies 50 and pads 124 invest at a topic proportional to the spring rate and disverse at the core proportional to the spring rate and disverse at a topic page.

As noted, the distance between the transducer assembles 50 is continuously measured by the point encoder 54 which is mechanically linked to the motion of the transducer assembles 60. Typically, the snooder uses a code siting mounted onto one of the carriages and an optical encoder reader mounted on the other carriage. As the distance between the transducers changes, the code siting moves between the site of the code of the carriage and the contraction of the carcion of the carriage and the contraction of the code and the optical reader reads the lines of the code siting set he lines are traversed.

The operation of the stepper motor 192 is controlled by controller 16 according to the quality of the signals received from the transducer assemblies 50 and positional data supplied by the position encoder.

Accordingly, the francticer drive mechanism £2 under the control of controller 16 provides automatips outlooming and other selectable functions. For example, the francticer drive mechanism separates the transducer 120 to allow the patients to be moved to and from a position between the transducers 120 without interference from the transducers solations the position chooder to a known transducer separation zero, extends the transducers 120 to a leaving or standing position, and secures the transducers 120 to a leaving or standing position, and secures the transducers 120 in a not or shipping position.

The controller t6 determines other parameters of interest, including broadband ultrasound attenuation

(BUA) and bone velocity, Also, the controller 16 calculates the speed of the ultrason is (gine) (SOS) through, for example, the using the distance between the transducers determined by the position encoder 54. The controller combines the results of the BUA and SOS measurements to obtain a bone mass measurement. Apparatus for measuring bone mass using ultrasound are known in the art. Such an apparatus is disclosed in, for example, United States Petant 4,774,959 to Paimer of al., which is incorporated herein in the entrely by refer-

The controller 19 uses temperature readings from temperature sensor 50 to improve the occuring of the position encoder measurements and correct for temperature dependent insecuracy in the utiliseature dependent insecuracy in the utiliseature dependent insecuracy in the utiliseature dependent served encoder sink playphing a temperature dependent term to the datas supplied by the position encoder 54. Additionally, the controller 16 applies as temperature dependent term to correct an estimation of the time delay through the delay in the 22 and the occuping part 124. Purthermore, the controller 16 uses the temperature dependent sensor that the controller 16 uses the temperature and the controller of the sensor delay within the special controller of the controller and the controller of the controll

Several features of the elastomer coupling pads 124 which provide efficient coupling of ultrasonic energy will now be described. The acoustic Impedance of the material of the pads 124 is matched to the acoustic impedance of human skin to provide a minimal loss of power and reduce extraneous reflections.

The coupling pade 124 also provide a waveguide function to colliment the accusite forean a sufficient distance along the propagation axis to allow the wavefronts at 50 evolve onto a more uniform intensity pattern. To this end, the accusical delay lines 122 are provided to allow the wavefronts to evolve from the granular near field pattern to a smoother far field pattern before entering the body.

The pads 124 are chosen to have a durometer corresponding to a sufficiently flexible waveguide that can partially conform to the shape of and provide some comfort to the patient. The shape of the pads 124 preferably conform to the heel so as to eliminate any air gaps between the heel and pad. The surfaces of the pads 124 which contact the transducers 120, the delay line, or the patent's skin may be shaped to expel air bubbles from the contact area when pressure is applied. The surface of the pad that contacts the patient's skin may be shaped 50 at an angle other than orthogonal to the propagation axis to reduce the acoustic reflection at the pad-to-skin interface by spreading the reflected energy over time and position. Other configurations of the pad also provide effective coupling of the ultrasonic energy. For example, 55 the pad may be conically shaped such that when the narrow portion of the conical shape engages the heel and is subsequently compressed, air is force from the

contact surface of the pad.

The material of the pads 124 is required to be compatible with coupling gel and non-irritating to the skin. One material of choice at this time is CIBA polyurethane (TDT 178-94) mixed with additive to provide a cured durometer of approximately 10 to 15 Shore A.

Commercially available coupling gel may be used between the skin and coupling pads. One implementation of the invention uses petroleum jelly as a coupling gel.

The ultrasound coupling gel that is commonly used to efficiently couple ultrasonic energy between the skin and transducers also may be eliminated by using a self wettling material such as Parker Laboratory Aqualitat pads. In one implementation of the design, self wetting coupling pads would be used as a disposable, or single used divide, eliminating concerns about sanhlation.

An alternative embodiment for the ultrasonic densitometric bone measuring unit is described in commonly owned U.S. Patent No. 5, 134,999 to Oslpov which is incorporated herein in its entirety by reference.

Referring to Fig. 13, an exemplary embodiment of an andributed (or stand alone) biochemical born emeating unit is shown. In this embodiment, the biochemical born emeasuring unit is shown. In this embodiment, the biochemical born emeasuring unit 160 includes a housing 162 which is preferably constructed for hard held operation. Typically, the housing is dimensioned shrillar to a hand held actualistor and includes a display 164, user operable switches 38 and 40, and an access port 186 for receiving a sample strip (described in more detail below). In the embodiment where the reader portion is disposable, screes port 186 is provided to facilitate the transfer through, for example capillary distribution, a bodily fluid sample onto a strip test. A printing page port 170 any optionally be provided to discharge a printout of the measured bone turnover data.

The stand alone biochemical bone measuring unit 160 is preferably a processor controlled unit powered by battery 172, seen in phantom in Fig. 3. Similar to the above described biochemical bone measuring unit, a controller 16 includes a microprocessor or microcontroller, memory (e.g., ROM and RAM), stored programs (e. g., system and application programs) for controlling the operation of the microprocessor or microcontroller, for performing a strip sample reading function, and for performing system verification procedures, such as selftest and calibration procedures. The controller 16 also includes input/output circuitry which permits the controller to interact with an alphanumeric display 22, a printer 20, control buttons 38 and 40, and strip sample reading circuit 24. The circuitry for the stand alone unit is similar to that shown in Fig. 3 and described above. A communication port 21, seen in Fig. 7, is provided to permit data communication between, for example, the biochemical bone measuring unit and an external computer.

The operation of the biochemical bone measuring unit of the stand alone embodiment is similar to the operation described above with regards to the integral unit. To activate the system verification procedures, either procedures, either control button may be depressed a predefined number control button may be depressed a predefined for unterview of times to perform the desired function. To illustrate, and out the control button 40 may be depressed three times in rapid succession which may cause a system self-rest procedure to be executed. Alternatively, a keypead may be substituted for the control buttons 38 and 40 and connected to the processor. Using the benefit of the processor. Using the benefit of the processor. Using the benefit of the processor. Using the value of the control button, or the keyped may have dedicated function keys which when depressed cause the execution of the desired function.

Preferably, in this embodiment the biochemical boor measuring unit 160 is configured to detect be presented to the presence of one or more analysis on a preformatted strip sample, as described above, the strip sample is typically the result of a quantitative in-vitro diagnostic strip test preformed in blood or urins. The strip sample can be measured, for example, as discussed in the emboding the preformed in the control of the control of

Referring now to Figs. 14-16, alternative embodiments of the bone measuring system are shown. In Fig. 14, the bone measuring system 10, described above, and one or more external computers 140 (e.g., a personal or laptop computer). As seen in Fig. 14, bone measuring system 10 is coupled to the computer 140 via communication port 144 and serial port 146. The communication port 144 is connected to controller 16 and is preferably configured for serial and/or parallel communications, e.g., RS-232 standard communications. In this configuration, the bone characteristic data determined by controller 16 can be downloaded to computer 140 for subsequent processing. Further, an operator can send instruction data to system 10 from computer 140. For example, computer 140 could be used to 35 send instructions to controller 16 to perform the biochemical assessment of bone characteristics (e.g., the strip sample measurement procedure), to perform the densitometric assessment of bone characteristics (e.g., the bone mass measuring procedure), and to instruct the controller 16 to transfer the measured data to the computer for subsequent processing. In this embodiment, the bone measuring system 10 includes the biochemical bone measuring unit 12 with the strip sample reading circuit 24 and the ultrasound bone measuring unit 14 in a single housing for use in, for example, a practitioner's office. The strip sample reading circuit 24 is similar to that described hereinabove and for clarity will not be repeated. The ultrasound bone measuring unit 14 includes the transducer assemblies 50, the position 50 encoder 54 and the stepper motor 132 which operate in a similar manner as described above. An operator interface 148 is located on the housing of the system 10 and may include a display, keyboard, printer access port and a beener

In Fig. 15, the bone measuring system illustrated includes a biochemical bone measuring unit 12 and an ultrasound bone measuring unit 14, each coupled to

computers 140 through for example a serial communication introface 146. Alternatively, data communications between the biochemical bone measuring unit, ultra-sound bone measuring unit and the computers may be across a local area network (e.g., ETHERNET or token ring), a wide area network (War) or using wireless data transmission techniques such as FF or infair are. In this embodiment, ach module is a separate unit having an independent controller 16 connected to the internal components described above. Each controller 16 controller 15 can be accorded to the communication of the components of the controller of the communication of the components of the controller and controller and such unit.

The embodiment of Fig. 16 is similar to the embodiment of Fig. 15 is oceapt that an x-ray based denicional-ris bone measuring unt 150 is used to measure bone density. The x-ray unit 150 may holide a controlled connected to an x-ray source and an x-ray defector and to communication crucitly which neceluse data from crucity which have been decided and controller, receives data from the x-ray data controller, receives data from the x-ray data to the main controller, receives data from the x-ray data to the main controller or processing. A suitable x-ray unit is the model QDR 4500 manufactured by Hologic Inc.

Figs. 17-19 provide various baseline, monitoring and projection format displays which may be displayed by computer 140. Fig. 17a provides an exemplary graph of baseline bone densitometric data defined by bone mineral density versus the age of a patient. Fig. 17b provides an exemplary graph of baseline biochemical marker data defined by biochemical marker concentration (representing bone resorption, formation or net bone turnover) compared to typical age matched reference levels. Fig. 18a provides an exemplary graph of serial bone densitometric data defined by bone mineral density versus the age of the patient which illustrates a rate of change between measurements. Fig. 18b provides an exemplary graph of serial baseline biochemical marker data defined by biochemical marker concentration (representing bone resorption, formation or net turnover) compared to the concentration at a follow-up visit, which illustrates a rate of change between measurements. Fig. 19 provides an exemplary dynamic graph of bone densitometric data and biochemical marker data which illustrates a baseline BMD value based on densitometric data and a slope representing a rate of increase or decrease in bone density which is based on baseline biochemical markers to provide a projected BMD value of the patient at a future age.

It will be understood that verious modifications can be made to the embodiments of the present invention herein disclosed without departing from the spirit and scope threnc? For example, various size housings continued to the continued of the continued of contemplated, as well as various type of transcitucious. Aurious eyes of mechanisms to move the transcitucious. Various eyesterns for detecting the concentration of analytics are also contemplated. For example, various eyesterns for detecting the concentration of 15

Cleims

1. A bone measuring system, which comprises:

a computer having data communication capability; a blochemical bone measuring unit coupled to said computer and configured to obtain bone characteristic data including bone turnover data from a strip sample and to transfer said bone

- talituria sity senifie en illustrariates acad obtie characteristic data to said computer, and a densitometric bone measuring unit coupled 26 to said computer and configured to measure bone characteristic data including bone mass data, and to transfer said bone characteristic data to said computer.
- The system according to claim 1, wherein said computer receives said bone characteristic data from said biochemical and densitometric bone measuring units and processes said bone characteristic data for subsequent graphical display.
- The system according to claim 1, wherein said biochemical bone measuring unit comprises:

at least one access port configured to receive 40 as strip sample or to clinicat a bodyli fluid sample onto a strip test to form the strip sample; or at least one strip test to form the strip sample; configured to fluid sample receifing circuitalligned relative to said at least one access port, and configured to direct light toward the strip sample, be detect light to exist the strip sample place, and generate detected sample data; and a processor coupled to said at least one strip sample reading circuit, said processor being configured to actuate said strip sample reading 20 configured to actuate said strip sample reading and to transfer said detected sample data; and to transfer said detected sample data; and to transfer said detected sample data; and to transfer said detected sample data to

- The system according to claim 1, wherein said biochemical bone measuring unit comprises;
 - a plurality of access ports each configured to

receive a strip sample or to direct a bodily fluid sample onto a strip test to form the strip sample; a plurality of strip sample reading circuits, wherein one of said plurality of strip samples is aligned relative to one of said plurality of access ports, each strip sample reading circuit being configured to direct light toward the strip sample, to detect light reflected by the strip sample and generate detected sample data; and a processor coupled to said plurality of strip sample reading circuits, said processor being configured to actuate each of said plurality of strip sample reading circuits, to receive said detected sample data for said plurality of strip sample reading circuits, and to transfer said detected sample data to said computer.

- The system according to claim 1, wherein said densitemetric bone measuring unit is an ultrasound bone measuring unit.
- The apparatus according to claim 5, wherein said ultrasound bone measuring unit comprises;

a housing having a support portion and a pair of transducer assemblies configured to move relative to each other such that when a body portion of a patient is positioned in said support portion said transducer assemblies are moved to contact the body portion."

a processor coupled to said transducer assemblies and configured to excite at least one of said transducer assemblies and to measure ultrasound signals that pass through the body portion.

- The system according to claim 6, wherein said support portion of said housing is configured to support a foot.
- The system according to claim 1, wherein said densitometric bone measuring unit is an x-ray based unit having an x-ray source, an x-ray detector and a controller.
- 9. A bone measuring system, which comprises:

a compact housing having a body support portion and at least one access port configured to receive a strip sample or to direct a bodily fluid sample onto a strip test located within said housing so as to form the strip sample;

a biochemical bone measuring unit located within said housing and including at least one strip sample reading circuit configured to direct light toward the strip sample, and to detect said light reflected by the strip sample and generate detected sample data;

a densitometric bone measuring unit located within said housing and associated with said body support portion, said densitometric bone measuring unit being configured to generate bone data; and

a processor located within said housing and coupled to said at least one stips sample reading circuit and said densitometric bone measuring unit, said processor being configured to receive said detected sample data and gener. To ask bone turnover data therefore, to receive said bone data from said densitometric bone measuring unit to determine bone density, and to provide as an output bone characteristic data representing the formation or receiption of the other testing to the control of the cont

- The system according to claim 9, wherein said output is displayed on a display mounted to said housing such that a display surface of said display is visible through said housing.
- 11. A bone measuring system, which comprises:
 - a compact housing having a support portion and at least one access port;
 - at loast one strip sample reading circuit located within said housing and configured to direct light toward a strip sample associated with said at least one access port, and to detect light reflected by the strip sample and generate detected sample data:
 - an ultrasound bone measuring device poeltion within said housing in association with said support portion, said ultrasound bone measuring device being configured to generate broadband ultrasound attenuation data and sneed of sound data: and
 - a processor located within said housing and coupled to said a least on early ample readunique to said a least on early a sample reading circuit and said ultreasund bone measuring
 device, said processor being configured to receive said detected earmple data and egenerate 45
 bone tumover data from said detected sample
 data, to reache said broadband bone attenuation (rate and speed of sound data from said
 ultrasound bone measuring device and determine bone mass, and to provide as an output 50
 bone characteristic data representing the formation or resoption of born eviative to current
 bone density so as to facilitate prejections of
 future bone characteristics.
- The system according to claim 11, wherein said output is displayed on a display mounted to said housing such that a display surface of said display is vis-

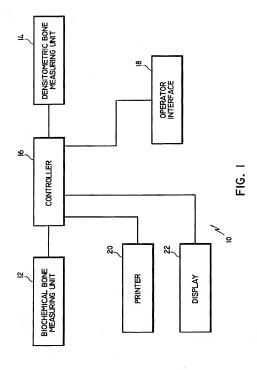
ible through said housing.

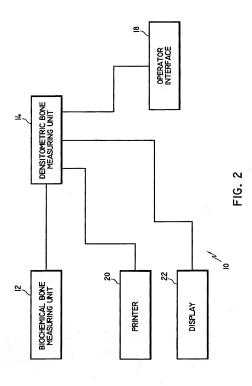
- A biochemical bone measuring unit for measuring bone characteristics from a strip sample, which comprises;
 - a housing having at least one access port; output means mounted to said housing for providing as an output bone turnover data;
- at least one strip sample reading circuit located within said housing realthy to said at least one access port and configured to direct light to a strip sample associated with said access port, and to detect light reflected by said strip sample and generate detected sample data therefrom; and
 - a processor located within said housing and oupled to said at least one stip sample reading circuit, said processor being configured to receive said detected sample signal and generate said bone tumover data from said detected sample data, and to output said bone turnover data through said output means.
- 5 14. The apparatus according to claim 13, wherein said output means comprises a communication port that provides data communication with an external device.
- within said housing and configured to direct 39 15. The apparatus according to claim 14, wherein said light toward a strip sample associated with said external device is a computer.
 - 16. The apparatus according to claim 13, wherein said output means comprises a display mounted to said housing such that a display surface of said display is visible through said housing.
 - The apparatus according to claim 13, wherein said housing is configured to be hand-held.
 - 18. The apparatus according to claim 13, wherein said at least one strip sample reading circuit incluses a light emitting source, an optical filter and a light remitting source, an optical filter and a light receiving element, said light emitting source being configured to emit light toward the strip sample, and said optical filter being configured to permit prodefined cofor wavelengths reflected from the strip sample to pass therethrough, and wherein said light detecting dement receives said filtered light and generates said sample obtacted data for transfer to said processor.
 - 19. The apparatus according to claim 18, wherein said at least one strip sample reading circuit includes a second optical filter and a second light detecting element, said second optical filter being configured to pass predefined color wavelengths of light reflected from a reference portion of the strip sample and said.

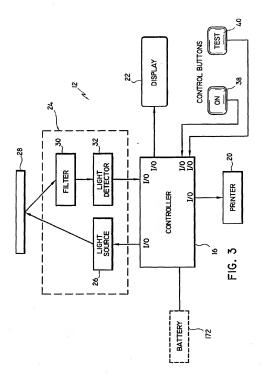
second light detecting element receives said filtered light and generates a reference signal for transfer to said processor.

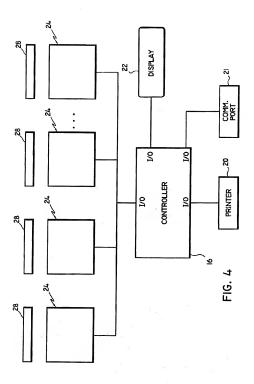
- The apparatus according to claim 18, wherein said 5 light emitting source is a diode.
- The apparatus according to claim 18, wherein said light emitting source is an incandescent lamp.
- 22. The apparatus according to claim 18, wherein said light emitting source is a fluorescent light source.
- 23. The apparatus according to claim 13, wherein said at least one stip sample reading circuit includes a 15 light emitting source, an optical filter and a light re-earling source and continued to the continued of the continued to emit light toward the strip sample, and said optical filter being confligured to permit fluorescent light emitted from the strip sample to pass 20 therefine out, and wherein said light detecting element receives said filtered light and generates said sample detected data for transfer to said processor.
- 24. A method for projecting bone characteristics of a 25 patient, comprising:
 - reading a strip sample by directing light toward the strip sample and detecting light reflected from the strip sample and generating signal data indicative of a predefined cotor wavelength for defining bone turnover data associated with the patient.
 - obtaining bone density data for the patient; and projecting future bone characteristics based on said bone density data and said bone turnover data
- teristic data, in which system or method the bone 40 characteristic data are obtained by use of a bio-chemical bone measuring until in combination with a destination bone measuring until in combination with a destination bone measuring until, and wherein, once the bone characteristic data are obtained, a determination of whether bone formation or bone 45 resorption is occurring is made and future bone characteristics are projected.

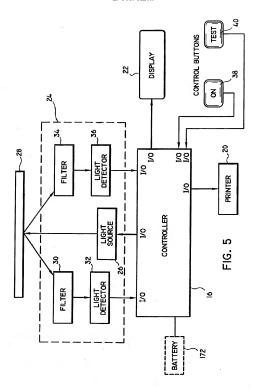
25. A system or method for determining bone charac-

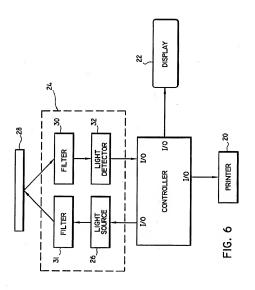


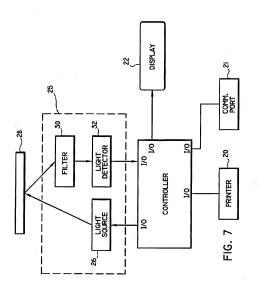


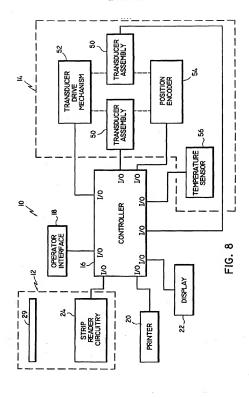


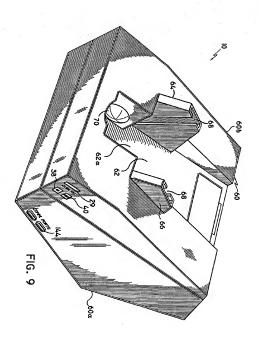




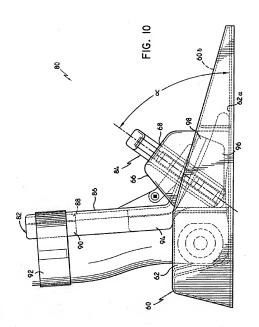


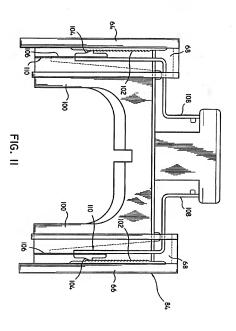




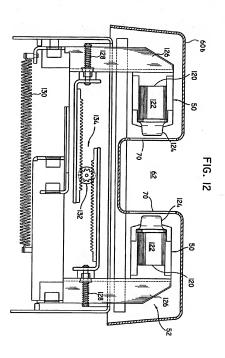


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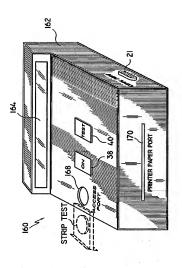
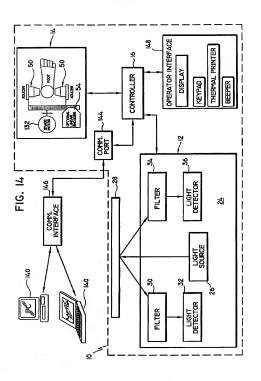


FIG. 13



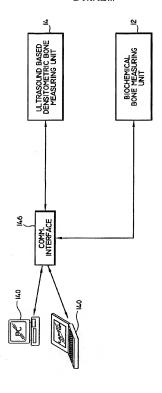


FIG. 15

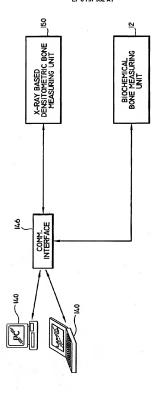


FIG. 16

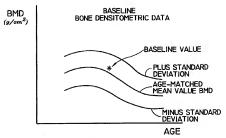
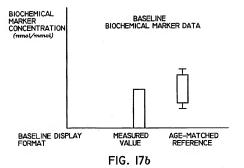
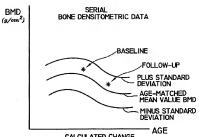


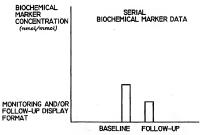
FIG. 17α





CALCULATED CHANGE
BETWEEN MEASUREMENTS = XX%

FIG. 18a



CALCULATED CHANGE BETWEEN MEASUREMENTS = XX%

FIG. 186

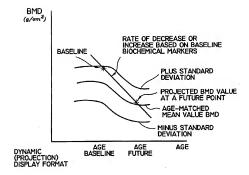


FIG. 19



European Paten

EUROPEAN SEARCH REPORT

Application Number EP 97 30 2116

	DOCUMENTS CONSI	DERED TO BE R	ELEVANT			
Category	Citation of document with it of relevant pa	edication, where appropriate	e, R	elevant chim	CLASSIFICATI APPLICATION	ON OF THE
Y A	O 96 04554 A (S.A.N.D. IMSTITUTE (AUST) TY. LIMITED) page 1, line 8 - page 3, line 27; claim 4; figures 1-4 *		13	2,5-7, ,16,17 11,24,		
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Y	EP 0 183 524 A (SYN PARTNERSHIP)	TEX DIAGNOSTIC	IMITED 13	,16,17	ĺ	
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A	US 5 132 097 A (R.A	•	11 13 18	4,9, -15, -22		
	* column 6, line 57 figures 1-8 *	- column 7, In	ne 39;		TECHNICAL	EIFI DS
D,A	US 4 811 373 A (J.#		1,	1,8	SEARCHED A61B	(Ist.Cl.4)
A	US 5 062 714 A (S.)			,18,	G01N	
	* column 3, line 43 - column 7, line 28; figures 1-20 *			,23		
	The present search report has			,	Freedor	_
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A. te	CATEGORY OF CITED OOCUME relicularly relevant if taken alone relicularly relevant if combined with an coment of the same cartegory theological background as-written disclosure	INTE T:	henry or principle un artier patent documenter the filling data locusment cited in the necessary cited for an member of the same	her reasons		
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